

<https://helda.helsinki.fi>

---

## A Theranostic Cellulose Nanocrystal-based Drug Delivery System with Enhanced Retention in Pulmonary Metastasis of Melanoma

Imlimthan, Surachet

2021-05-06

---

Imlimthan , S , Khng , Y-C , Keinänen , O , Zhang , W , Airaksinen , A , Kostiainen , M A , Zeglis , B M , Santos , H A & Sarparanta , M 2021 , ' A Theranostic Cellulose Nanocrystal-based Drug Delivery System with Enhanced Retention in Pulmonary Metastasis of Melanoma ' , Small , vol. 17 , no. 18 , 2007705 . <https://doi.org/10.1002/smll.202007705>

---

<http://hdl.handle.net/10138/330326>

<https://doi.org/10.1002/smll.202007705>

---

cc\_by\_nc

---

*Downloaded from Helda, University of Helsinki institutional repository.*

*This is an electronic reprint of the original article.*

*This reprint may differ from the original in pagination and typographic detail.*

*Please cite the original version.*

# A Theranostic Cellulose Nanocrystal-Based Drug Delivery System with Enhanced Retention in Pulmonary Metastasis of Melanoma

Surachet Imlimthan, You Cheng Khng, Outi Keinänen, Wenzhong Zhang, Anu J. Airaksinen, Mauri A. Kostiaainen, Brian M. Zeglis, Hélder A. Santos, and Mirkka Sarparanta\*

Metastatic melanoma can be difficult to detect until at the advanced state that decreases the survival rate of patients. Several FDA-approved BRAF inhibitors have been used for treatment of metastatic melanoma, but overall therapeutic efficacy has been limited. Lutetium-177 ( $^{177}\text{Lu}$ ) enables simultaneous tracking of tracer accumulation with single-photon emission computed tomography and radiotherapy. Therefore, the codelivery of  $^{177}\text{Lu}$  alongside chemotherapeutic agents using nanoparticles (NPs) might improve the therapeutic outcome in metastatic melanoma. Cellulose nanocrystals (CNC NPs) can particularly deliver payloads to lung capillaries in vivo. Herein,  $^{177}\text{Lu}$ -labeled CNC NPs loaded with vemurafenib ( $^{177}\text{Lu}$ ]Lu-CNC-V NPs) is developed and the therapeutic effect in BRAF V600E mutation-harboring YUMM1.G1 murine model of lung metastatic melanoma is investigated. The  $^{177}\text{Lu}$ ]Lu-CNC-V NPs demonstrate favorable radiolabel stability, drug release profile, cellular uptake, and cell growth inhibition in vitro. In vivo biodistribution reveals significant retention of the  $^{177}\text{Lu}$ ]Lu-CNC-V NPs in the lung, liver, and spleen. Ultimately, the median survival time of animals is doubly increased after treatment with  $^{177}\text{Lu}$ ]Lu-CNC-V NPs compared to control groups. The enhanced therapeutic efficacy of  $^{177}\text{Lu}$ ]Lu-CNC-V NPs in the lung metastatic melanoma animal model provides convincing evidence for the potential of clinical translation for theranostic CNC NP-based drug delivery systems after intravenous administration.


## 1. Introduction

Metastatic melanoma is the most aggressive form of skin cancer, and patients with the disease continue to have a poor prognosis after treatment.<sup>[1–3]</sup> Metastatic melanoma develops through the dissemination of melanoma cells from the primary tumor site to different parts of the body (e.g., lung, liver, spleen, and kidney) via the circulatory and lymphatic systems.<sup>[4,5]</sup> In clinical practice, there are several options for the treatment of metastatic melanoma, including immunotherapy, radiation therapy, and chemotherapy.<sup>[3]</sup> In melanoma, the serine/threonine protein kinase BRAF plays a critical role in growth signaling transduction in the mitogen-activated protein kinase (MAPK) pathway.<sup>[6–8]</sup> Over 90% of tumorigenic BRAF mutations appear at codon 600 (V600E), where an  $\alpha$ -amino acid (valine; V) position in the protein kinase domain is substituted by glutamic acid (E).<sup>[9,10]</sup> Kinase activity in melanomas harboring

S. Imlimthan, Y. C. Khng, Dr. O. Keinänen, Dr. W. Zhang,  
Prof. A. J. Airaksinen, Dr. M. Sarparanta  
Department of Chemistry  
University of Helsinki  
Helsinki FI-00014, Finland  
E-mail: mirkka.sarparanta@helsinki.fi

Dr. O. Keinänen, Prof. B. M. Zeglis  
Department of Chemistry  
Hunter College  
The City University of New York  
New York, NY 10021, USA

Dr. O. Keinänen, Prof. B. M. Zeglis  
Department of Radiology  
Memorial Sloan Kettering Cancer Center  
New York, NY 10021, USA

 The ORCID identification number(s) for the author(s) of this article can be found under <https://doi.org/10.1002/smll.202007705>.

© 2021 The Authors. Small published by Wiley-VCH GmbH. This is an open access article under the terms of the Creative Commons Attribution-NonCommercial License, which permits use, distribution and reproduction in any medium, provided the original work is properly cited and is not used for commercial purposes.

DOI: 10.1002/smll.202007705

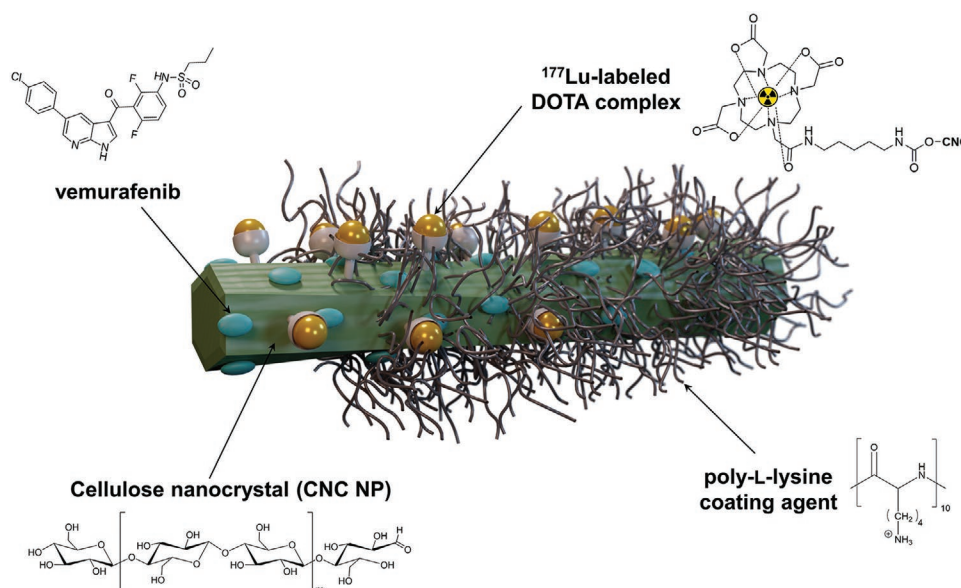
Prof. A. J. Airaksinen  
Turku PET Centre  
Department of Chemistry  
University of Turku  
Turku FI-20521, Finland

Prof. M. A. Kostiaainen  
Biohybrid Materials  
Department of Bioproducts and Biosystems  
Aalto University  
Aalto FI-00076, Finland

Prof. B. M. Zeglis  
Ph.D. Program in Chemistry  
Graduate Center of the City University of New York  
New York, NY 10016, USA

Prof. B. M. Zeglis  
Department of Radiology  
Weill Cornell Medical College  
New York, NY 10021, USA

Prof. H. A. Santos  
Drug Research Program  
Division of Pharmaceutical Chemistry and Technology  
Faculty of Pharmacy  
University of Helsinki  
Helsinki FI-00014, Finland



**Figure 1.** Schematic representation of the  $^{177}\text{Lu}$ -labeled CNC NPs loaded with vemurafenib ([ $^{177}\text{Lu}$ ]Lu-CNC-V NPs). The green rod represents a cotton cellulose nanocrystal (CNC NP). The bifunctional radiometal chelator DOTA- $\text{NH}_2$  is conjugated on the CNC surface via CDI-activated OH groups and further radiolabeled with  $^{177}\text{Lu}$ . Vemurafenib is entrapped on the surface of CNC by electrostatic interaction with the aid of poly-L-lysine as a capping agent.

the BRAF V600E mutation is elevated 500- to 700-fold compared to wild-type BRAF, leading to cell transformation and tumor formation.<sup>[11]</sup> In addition, the BRAF V600E mutation is found in 40–60% of melanoma patients, rendering it a promising candidate for targeted therapy.<sup>[12]</sup> PLX4032 (vemurafenib) is a clinically approved tyrosine kinase inhibitor that inhibits ATP binding in BRAF V600E-mutated melanomas, resulting in the deactivation of the MAPK pathway and reduction in cell proliferation and survival.<sup>[13,14]</sup> However, the therapeutic efficacy of vemurafenib remains suboptimal due to the need for high doses, poor bioavailability of the drug, adaptive drug resistance behavior, and the reactivation of the MAPK pathway from drug-induced stress responses after repeated cycles of treatment.<sup>[14–17]</sup>

Radiolabeled tracers have been applied in oncology for diagnosis, staging, therapy, and long-term monitoring of numerous cancers.<sup>[18]</sup> Lutetium-177 ( $^{177}\text{Lu}$ ) is a theranostic radionuclide that is frequently used in the clinic due to physical and nuclear properties—a relatively long half-life ( $t_{1/2} = 6.6$  d) and the emission of both gamma ( $\gamma$ ) and beta ( $\beta^-$ ) radiation—that enable simultaneous imaging and radiotherapy. The emission of gamma radiation ( $E_\gamma = 208$  keV, 10% intensity) facilitates noninvasive diagnostic imaging using single-photon emission computed tomography (SPECT). The  $\beta^-$  radiation ( $E_{\beta_{\text{max}}} = 0.498$  MeV, 79% intensity) enables endoradiotherapy through the deposition of ionizing particles that induce cytotoxic ROS formation and DNA double-strand breaks within the cells.<sup>[19,20]</sup>

Nanostructured materials have been employed in the field of nanomedicine as drug delivery systems (DDS) intended to address the limitations in conventional formulations.<sup>[21,22]</sup> Nanoparticles (NPs) are a versatile platform that can be tailored to have the desired characteristics and properties for specific

drug delivery applications. Engineered NPs offer several advantages, including improved drug solubility, controlled drug release, increased drug circulation half-life, and enhanced targetability.<sup>[23–25]</sup> Cellulose is an abundant biomacromolecular material obtained from various renewable resources.<sup>[26,27]</sup> In drug delivery applications, nanocrystalline cellulose nanoparticles (CNC NPs) have received great interest as a biopolymer-based nanomaterial that can be easily and economically prepared from the separation of the crystalline regions of native cellulose through strong acid hydrolysis.<sup>[28,29]</sup> The CNC NPs possess versatile physical and chemical properties, including a needle-like structure with dimensions of 5–10 nm in width and 100–300 nm in length (for CNC NPs derived from wood and cotton), a high aspect ratio (length/width), and surface chemistry that is amenable to conjugation via the manipulation of hydroxyl (OH), aldehyde (CHO), and sulfate (OSO<sub>3</sub>) groups.<sup>[29,30]</sup> Furthermore, the biocompatibility, biodegradability, and lack of toxicity of CNC NPs has led many to advocate their use in biomedical applications.<sup>[31–35]</sup> According to our previous reports,<sup>[31,35]</sup> radiolabeled CNC nanoparticles display a transient uptake and retention in the lung tissue, suggesting that rod-shaped CNC NPs could be used to target the pulmonary vasculature as they tumble close to the wall of the blood vessels and could potentially embolize into neovascularization of the metastatic tumors.<sup>[36]</sup> Since CNC NPs tend to accumulate in the lung vasculature, the delivery of vemurafenib with CNC NPs to metastatic melanoma in the lung is an attractive model to explore the drug delivery potential of the CNC NPs to lung tissue. Furthermore, the CNC NPs can be readily radiolabeled with the theranostic radioisotope  $^{177}\text{Lu}$  to explore the potential synergistic or added effects of  $^{177}\text{Lu}$ -radiotherapy and vemurafenib chemotherapy.

In this study, we developed theranostic  $^{177}\text{Lu}$ -labeled CNC NPs loaded with vemurafenib ([ $^{177}\text{Lu}$ ]Lu-CNC-V NPs, **Figure 1**) and investigated their biological behavior in both murine and human melanoma cell models and animals bearing metastatic

Prof. H. A. Santos  
Helsinki Institute of Life Science (HiLIFE)  
Helsinki FI-00014, Finland

melanoma allografts in the lung. The theranostic CNC NPs were prepared through the conjugation of 1,4,7,10-tetraazacyclododecane-1,4,7,10-tetraacetic acid (DOTA) to the hydroxyl groups on the surface of the CNC NPs followed by radiolabeling with  $^{177}\text{Lu}$ . Then, vemurafenib was incorporated onto the surface of the  $^{177}\text{Lu}$ -labeled CNC NPs via the electrostatic interactions using a cationic polymer (poly-L-lysine) as a capping agent. The in vitro radiolabeling stability and drug release profiles of the  $^{177}\text{Lu}$ -CNC-V NPs were studied in different physiological simulated conditions. Furthermore, the cell cytotoxicity, cellular uptake, and clonogenic cell survival were evaluated in both murine and human melanoma cell models. Finally, the ex vivo biodistribution and therapeutic studies of the  $^{177}\text{Lu}$ -CNC-V NPs were assessed in mice bearing YUMM1.G1 lung metastatic melanoma allografts for preclinical evaluation of the theranostic CNC NP-based DDS and its potential of future clinical translation.

## 2. Results and Discussion

### 2.1. Materials Characterization

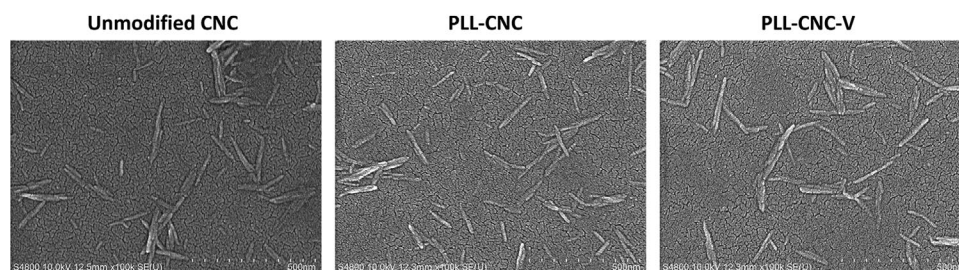
The DOTA-modified CNC NPs were successfully prepared through the CDI-mediated amidation reaction between the activated hydroxyl groups and DOTA-NH<sub>2</sub>. When compared to unmodified CNC spectrum, the ATR-FTIR spectrum of the DOTA-CNC NPs contained the conjugation product peaks, including the amide II band (C–N stretching and N–H bending) at 1510–1700 cm<sup>−1</sup>, and alkyl band (C–H stretching) at 2850–2950 cm<sup>−1</sup>, demonstrating successful conjugation of DOTA chelator to the surface of the CNC NPs (Figure S1, Supporting Information). Moreover, the changes in the C, H, and N compositions of modified CNC NPs corroborated the successful conjugation reaction. While there was no significant difference in the C and H content from that of unmodified CNC NPs, the amount of N increased substantially to approximately 0.9% in the DOTA-CNC NPs, presumably due to the presence of the N in the DOTA macrocyclic ring (Table S1, Supporting Information). The N content was further used to estimate the degree of substitution (DS), providing the average number of DOTA molecules attached per monomeric unit of the CNC NPs (Supporting Information). The DS of DOTA molecules to the CNC NPs was approximately 0.24, which is in agreement with the values reported in the literature where the DS of grafting molecules on the cellulose surface through heterogeneous reactions is generally less than 1.0 as a result of an unreactive

hydroxyl group at the carbon position C2 and C3 of the anhydroglucose unit.<sup>[37]</sup> The DOTA-CNC NPs showed an increase in zeta ( $\zeta$ )-potential value ( $-30.67 \pm 0.91$  mV) compared to the native CNC NPs ( $-52.53 \pm 2.67$  mV). However, the negative surface charge of the DOTA-modified CNC NPs is sufficiently low to avoid nonspecific adsorption of plasma proteins.<sup>[38]</sup> Upon capping with PLL, the  $\zeta$ -potential reversed to positive ( $47.23 \pm 1.26$  mV) and was lowered to close to 0 mV ( $1.72 \pm 0.27$  mV) in the full  $^{177}\text{Lu}$ -radiolabeled  $^{177}\text{Lu}$ -CNC-PLL-V nanotheranostic construct. Compared to neutral or negatively charged nanoparticles, positively charged nanoparticles have a stronger interaction with the negatively charged cell membrane driven by electrostatic attraction. The slightly positive charge of  $^{177}\text{Lu}$ -CNC-PLL-V NPs might favor the cell adhesion both in vitro and in vivo, leading to higher accumulation within cells.<sup>[39]</sup> The  $\zeta$ -potential results of all nonradiolabeled and radiolabeled CNC NPs in this work are compiled in Table S2, Supporting Information. In addition, FE-SEM images were acquired to determine the morphology of the CNC NPs after the chemical modifications. There is no dramatic change in the morphology of the modified CNC NPs compared to unmodified CNC NPs, and all the CNC NPs demonstrated a rod-like shape with an average width of 9–14 nm and length of 136–158 nm as well as a uniform particle size distribution (Figure 2 and Figure S2, Supporting Information).

### 2.2. $^{177}\text{Lu}$ -Radiolabeled CNC NPs and In Vitro Stability

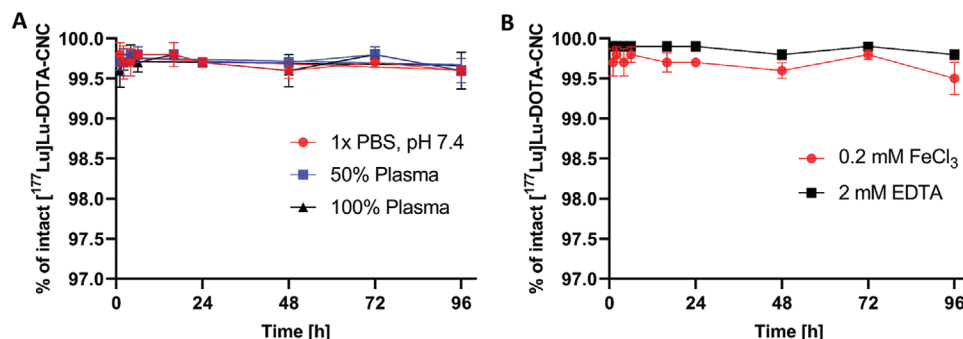
The DOTA-CNC NPs were successfully labeled with  $^{177}\text{Lu}$  using standard radiolabeling procedures with a decay-corrected radiochemical yield (RCY =  $74 \pm 2\%$ ,  $n = 4$ ) and a radiochemical purity (RCP > 99.5%) after purification. The in vitro stability of  $^{177}\text{Lu}$ -radiolabeled CNC construct was thoroughly studied in various simulated physiological conditions, including 1× PBS (pH 7.4), and 50% and 100% human plasma. The stability of the radiometal–ligand complex was also investigated using  $0.2 \times 10^{-3}$  M FeCl<sub>3</sub> and  $2 \times 10^{-3}$  M EDTA as a competing metal and ligand, respectively.

In general, the  $^{177}\text{Lu}$ -CNC NPs demonstrated good radiolabel stability with >99.5% of the  $^{177}\text{Lu}$  radiolabel remaining bound to the surface of the CNC NPs after 96 h of incubation in 1× PBS (pH 7.4), and in 50% and 100% human plasma in 1× PBS (pH 7.4) at 37 °C (Figure 3A). The results suggest that plasma proteins have no significant effect on the radiolabel complex stability or nanomaterial degradation, indicating



**Figure 2.** FE-SEM images of unmodified CNC NPs, PLL-coated CNC (PLL-CNC) NPs, and vemurafenib-loaded CNC (PLL-CNC-V) NPs, scale bar = 500 nm.





**Figure 3.** The in vitro stability of  $^{177}\text{Lu}$ -radiolabeled CNC NPs in A) 1x PBS (pH 7.4), and in 50% and 100% human plasma in 1x PBS (pH 7.4), and B)  $0.2 \times 10^{-3} \text{ M}$   $\text{FeCl}_3$  and  $2 \times 10^{-3} \text{ M}$  EDTA challenges. The values represent mean  $\pm$  s.d. ( $n = 3$ ).

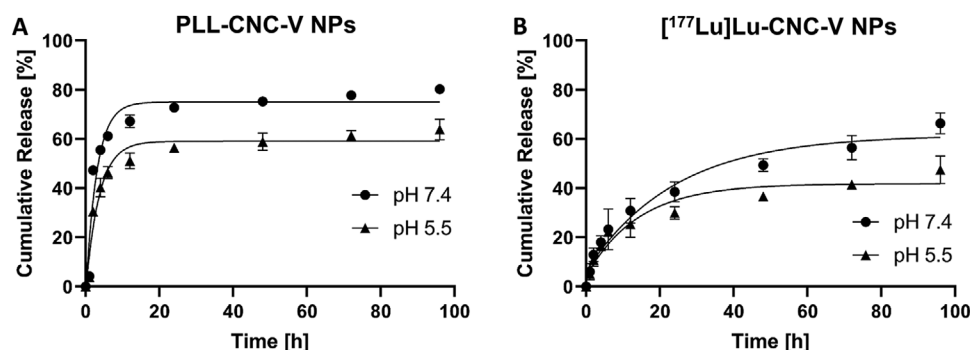
suitability for in vivo use. Moreover, the  $^{177}\text{Lu}$ -CNC NPs revealed remarkable complex stability ( $\geq 99.5\%$  intact) over 96 h of incubation in  $0.2 \times 10^{-3} \text{ M}$   $\text{FeCl}_3$  solution where the  $\text{Fe}^{3+}$  concentration was considerably higher than the normal range ( $10\text{--}30 \times 10^{-6} \text{ M}$ ) in human tissues.<sup>[40]</sup> Similarly, the percentage of intact  $^{177}\text{Lu}$ -DOTA-CNC NPs in  $2 \times 10^{-3} \text{ M}$  EDTA solution was maintained at 99.8% over the incubation period, which indicates stable coordination of the  $^{177}\text{Lu}$  in the DOTA chelator (Figure 3B).

### 2.3. Drug-Loaded CNC NPs and In Vitro Drug Release Profiles

Vemurafenib was successfully loaded to both nonradiolabeled and radiolabeled CNC NPs through noncovalent binding on the surface of the CNC in the presence of cationic PLL as a capping agent, promoting the electrostatic binding of the hydrophobic drug. The nonradiolabeled PLL-CNC-V NPs showed a moderate drug loading efficiency of  $13.13 \pm 1.00\%$ , while the loading efficiency on the radiolabeled  $^{177}\text{Lu}$ -CNC-V NPs ( $29.50 \pm 3.50\%$ ) was improved about twofold (Table S3, Supporting Information). This might be the result of a higher positive surface charge of  $^{177}\text{Lu}$ -CNC NPs compared to nonradiolabeled CNC NPs (Table S2, Supporting Information). The additional negative charge from the deprotonated carboxylic acid residues on the DOTA chelator of  $^{177}\text{Lu}$ -CNC-V NPs could promote the capping with PLL, which may drive a greater amount of vemurafenib to entrap on the surface of the CNC

in radiolabeled particles. Moreover, the obtained drug loading efficiency and loading degree of nonradiolabeled CNC NPs in this work were slightly lower than those reported for the CNC NP-based DDS in the literature, in which the average loading efficiency and loading degree for hydrophobic compounds have ranged between 21–25% and 14–20%, respectively.<sup>[41–43]</sup>

The ability of the developed CNC NPs DDS to release the vemurafenib payload was first evaluated in physiological fluids in vitro, including 1x PBS (pH 7.4) and  $10 \times 10^{-3} \text{ M}$  acetate buffer (pH 5.5) for blood and tumor microenvironment mimicking conditions, respectively. Overall, both PLL-CNC-V NPs and the  $^{177}\text{Lu}$ -CNC-V NPs exhibited a rapid release pattern of vemurafenib after 2 h of incubation in both simulated media before the release kinetics were sustained over the incubation period (Figure 4). Interestingly, both NP constructs demonstrated superior drug release rate in 1x PBS (pH 7.4) in which the cumulative release reached 80% and 66% while only 64% and 47% were attained at pH 5.5 after 96 h of incubation for PLL-CNC-V NPs and  $^{177}\text{Lu}$ -CNC-V NPs, respectively. This phenomenon could be explained by the fact that the PLL coated on the surface of CNC is bound by electrostatic interactions. A strong electrolyte of  $137 \times 10^{-3} \text{ M}$  NaCl in PBS buffer might screen some electrostatic interactions and weaken the binding of PLL, resulting in loss of the capping capacity. Furthermore, the 10% (v/v) human serum added to the incubation media in order to induce a sink condition could promote the scavenging of the PLL coating due to electrostatic interactions with the serum proteins.



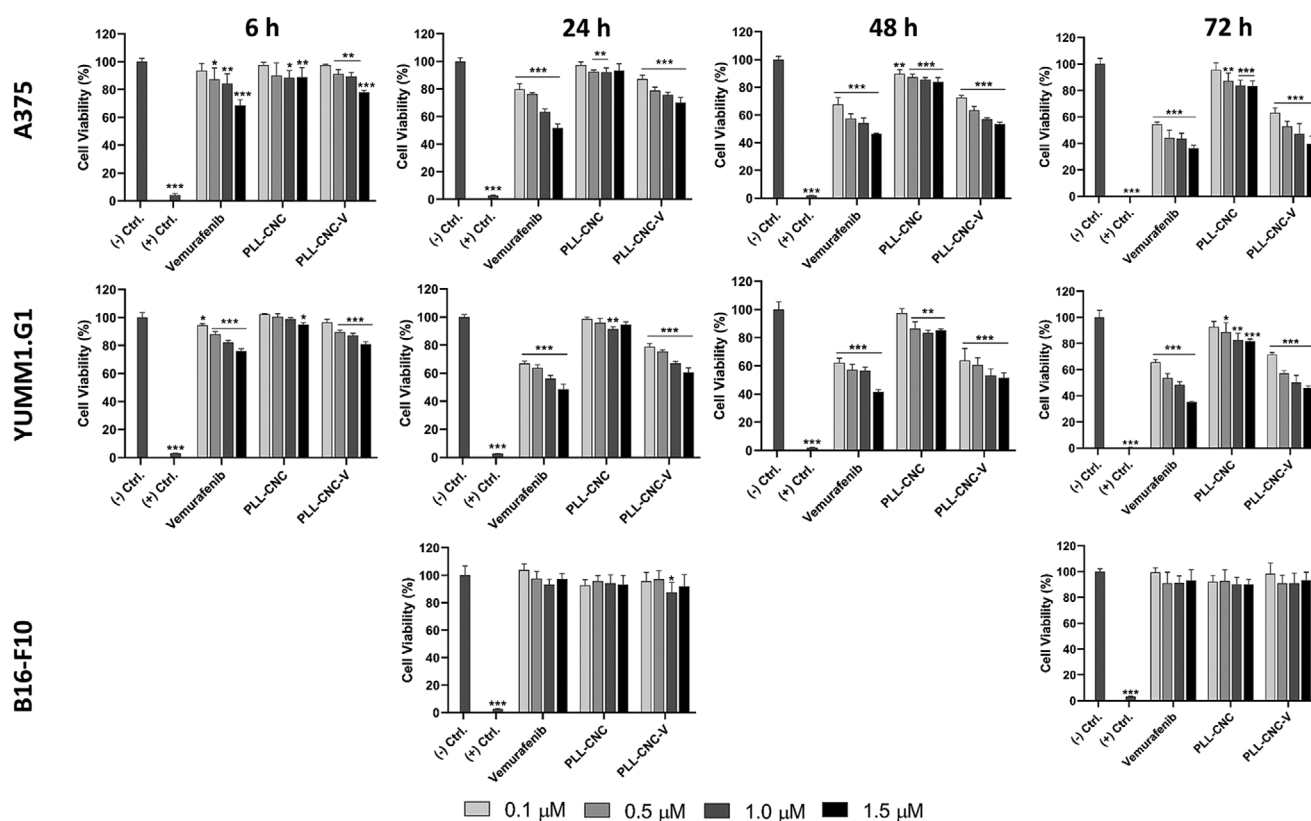
**Figure 4.** In vitro drug release profiles of A) vemurafenib-loaded nonradiolabeled PLL-CNC-V NPs and B) vemurafenib-loaded radiolabeled  $^{177}\text{Lu}$ -CNC-V NPs in simulated physiological 1x PBS (pH 7.4) and condition mimicking the tumor microenvironment (pH 5.5, representing the late endosome) over 96 h. The values represent mean  $\pm$  s.d. ( $n = 3$ ).

In contrast, the release profiles of the [ $^{177}\text{Lu}$ ]Lu-CNC-V NPs in both conditions were decelerated compared to the nonradioactive PLL-CNC-V NPs. This might be the influence from the carboxylic residues on the nonradiolabeled DOTA chelator left on the surface of the [ $^{177}\text{Lu}$ ]Lu-CNC-V NPs after radiolabeling. The negative charge from the carboxylic groups might foster an interaction with vemurafenib while PLL starts to lose its capping capacity, leading to a slower drug release pattern. Therefore, the drug loading strategy and coating materials for surface stabilization could be further optimized to enhance the capping capacity and minimize the release at physiological pH 7.4 while triggering a burst release at the acidic pH of the tumor microenvironment. Regardless of the room for improvement, the results demonstrate that both non-radiolabeled and radiolabeled CNC NPs are promising nanocarriers for the delivery of vemurafenib with satisfactory release behavior for in vivo use.

## 2.4. In Vitro Cytocompatibility

Despite the promising radiolabeling yield, radiolabel stability and drug release pattern of the CNC NPs, the cytotoxicity of the newly developed vemurafenib-loaded CNC NPs is an important issue that needs to be investigated before in vivo applications.

The in vitro cytotoxicity screening test could provide preliminary information on the potential toxicity and subcellular targeting of drug-loaded nanoparticles that could suggest a prediction of in vivo effects. The in vitro cytotoxicity of the PLL-CNC-V NPs was studied in both BRAF V600E mutant cell lines (murine YUMM1.G1 and human A375) and wild-type BRAF cell line (murine B16-F10) at various concentrations and incubation times. In general, the YUMM1.G1 and A375 cell lines exhibited a linear decrease in cell viability when incubated with either free vemurafenib or PLL-CNC-V NPs at increasing concentrations over time (Figure 5). The PLL-CNC-V NPs were less cytotoxic than free vemurafenib in both cell lines up to 24 h of incubation, suggesting the capability of CNC NPs to sustain the release of vemurafenib over time before the cytotoxic effect became similar at 48 h and 72 h of incubation (Table S4, Supporting Information). Moreover, the downstream effects of BRAF inhibition in YUMM1.G1 and A375 cell lines were corroborated with western blot showing that MEK phosphorylation was successfully inhibited with the increase in vemurafenib concentration (Figure S3, Supporting Information) in both of the cell lines. As expected, the PLL-CNC NPs (empty nanosystem) showed no significant cytotoxic effect at any of the concentrations up to 48 h of incubation, which was in accordance with our previous reports.<sup>[31,32]</sup> However, a slight decrease in cell



**Figure 5.** In vitro cell viability studies in BRAF V600E expressing cell lines (human A375 and murine YUMM1.G1 melanoma) and wild-type BRAF expressing melanoma cell line (murine B16-F10) after incubation with free vemurafenib, PLL-CNC NPs, and PLL-CNC V NPs at vemurafenib concentrations of  $0.1 \times 10^{-6}$ ,  $0.5 \times 10^{-6}$ ,  $1.0 \times 10^{-6}$ , and  $1.5 \times 10^{-6}$  M with respective CNC concentrations of 0.5, 2.2, 4.5, and  $6.7 \mu\text{g mL}^{-1}$  for 6, 24, 48, and 72 h. For B16-F10 the assay was carried out only at 24 and 72 h. The negative (–) and positive (+) controls for cell viability were fresh cell culture media and 1% (v/v) Triton X-100 solution, respectively. The statistical analysis was carried out using the unpaired Student's *t*-test in comparison with the negative control where the significant differences were set at \**p* < 0.05, \*\**p* < 0.01, and \*\*\**p* < 0.001. Columns represent the mean  $\pm$  s.d. (*n* = 4).

viability (<90%) was observed at 4.5 and 6.7  $\mu\text{g mL}^{-1}$  concentrations after 72 h of incubation in both cell lines. This might be due to the potential cytotoxicity induced by the cationic charge of PLL after long exposure time with the cells. Additionally, in order to further corroborate that the cytotoxic effects were primarily arising from the vemurafenib release and effects in the BRAF V600E mutant cell lines, the cytotoxicity of the constructs was assayed in the murine BRAF wild-type B16-F10 melanoma cell line at 24 and 72 h representing medium and long exposure times. The proportion of viable B16-F10 cells stayed over 90% for all conditions, concentrations and time points. Therefore, the overall results indicate the potential to use of the CNC NPs as a nanocarrier to delivery and sustained release of vemurafenib to tumor cells expressing the BRAF V600E mutation in vivo, while the construct remains safe for nontarget cells expressing wild-type BRAF.

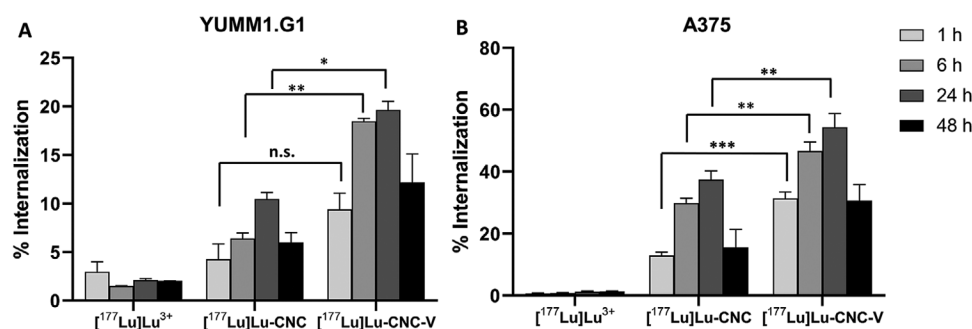
## 2.5. Cellular Uptake Studies

The internalization of NPs into the cells is often needed for successful transportation and accumulation of active molecules (e.g., drugs, DNA, RNA, and imaging agents) to specific intracellular sites. The cellular uptake of nontargeted NPs is usually through the endocytosis pathway and penetration at the lipid bilayer on the cell membrane, however, other internalization pathways can be regulated for targeted NPs, such as ion channels, receptors, and transporters.<sup>[44]</sup> The uptake mechanisms of NPs vary depending on size, uniformity of the size distribution, shape, and surface properties. Typically, the internalization in cells is qualitatively determined through the visualization of the signal from a fluorescent dye tagged on the surface of NPs using fluorescence microscopy. However, the internalization of the  $^{177}\text{Lu}$ -radiolabeled CNC constructs in this work is conveniently evaluated through the quantitative detection of gamma radiation from the  $^{177}\text{Lu}$  accumulated within the cells. The results showed that there was no substantial accumulation of free  $^{177}\text{LuLu}^{3+}$  in either YUMM1.G1 or A375 cell lines while an increase in internalized radioactivity within the cells was observed with the  $^{177}\text{LuLu}$ -CNC NPs and  $^{177}\text{LuLu}$ -CNC-V NPs over time (Figure 6). Both radiolabeled CNC NPs revealed a linear trend of radioactivity accumulation in both cell lines

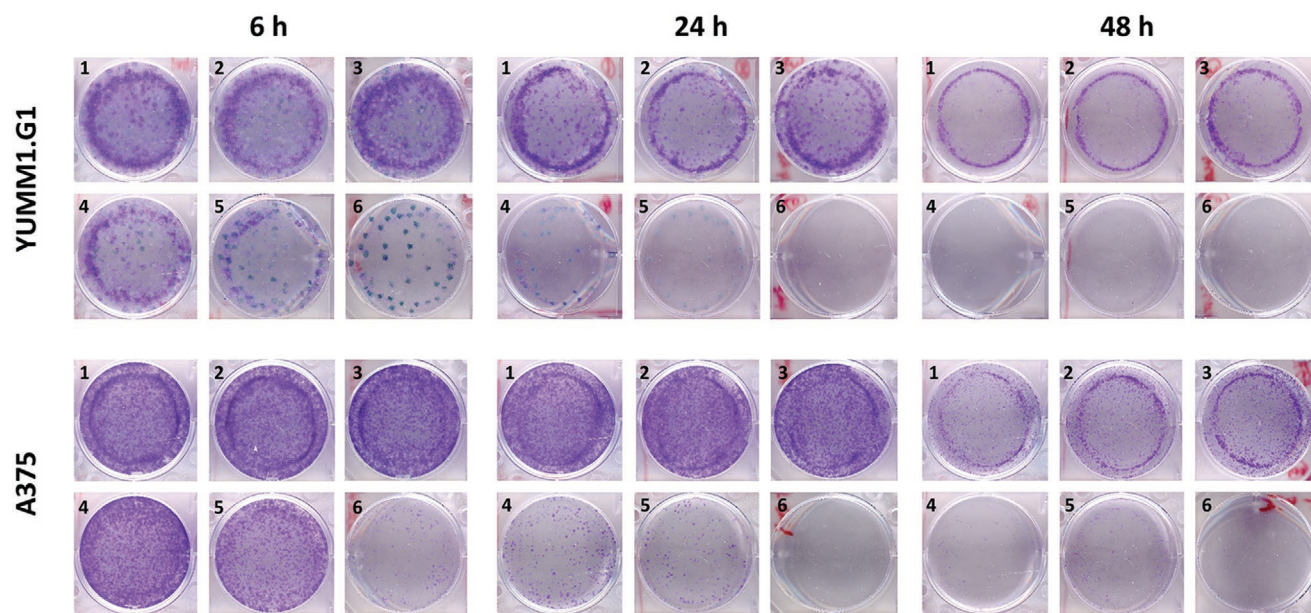
up to 24 h of incubation. Furthermore,  $^{177}\text{LuLu}$ -CNC-V NPs exhibited a higher uptake in both cell lines compared to the  $^{177}\text{LuLu}$ -CNC NPs with double the internalization at all time points. A greater degree of internalization of the  $^{177}\text{LuLu}$ -CNC-V NPs could be a result of the positive surface charge of the NPs (Table S2, Supporting Information), which possibly stimulates a strong interaction with the negatively charged cell membrane. Surprisingly, both the CNC NPs tend to accumulate in human A375 melanoma cells with approximately three times higher uptake than in murine YUMM1.G1 melanoma cells at all time points. Unlike spherical NPs, the interaction and internalization mechanisms of rod-shaped NPs, especially the CNC NPs in this work are not completely elucidated and could rely on different factors, including physicochemical properties of the NPs, the cell type, membrane-wrapping energy consumption, activity of endocytosis pathways, and uptake behavior.<sup>[45]</sup> Moreover, the decrease of internalization after 48 h of incubation was noticed in both the radiolabeled CNC NPs in both tested cell lines. This is likely a result of the cytotoxic effect after long exposure during which the dead cells start to detach from the surface of the culturing plate. The detached cells with their accumulated radioactivity are potentially washed out to the unbound fraction, complicating the determination of the internalized activity at time points beyond 24 h.

## 2.6. Clonogenic Cell Survival

Clonogenic assays are commonly used to investigate the ability of cells to proliferate after exposure to ionizing radiation that induces DNA damage and cell apoptosis, but it is also useful for investigation of the combination of radiation with other treatment modalities.<sup>[46]</sup> In this experiment, the clonogenic cell survival in YUMM1.G1 and A375 cells was explored after treatments with PLL-CNC NPs, free vemurafenib, free  $^{177}\text{LuLu}^{3+}$ ,  $^{177}\text{LuLu}$ -CNC NPs, and  $^{177}\text{LuLu}$ -CNC-V NPs for 6, 24, and 48 h to examine the effects of the chemoradiotherapeutic combination of the  $^{177}\text{LuLu}$ -CNC-V NPs and the individual nanotheranostic components (Figure 7). As the colonies formed by both cell lines tended to clump together, the plating efficiency and surviving fraction could not be accurately determined. Therefore, the discussion of results herein is simplified as a



**Figure 6.** Cellular uptake of radioactivity after incubation with free A)  $^{177}\text{LuLu}^{3+}$ ,  $^{177}\text{LuLu}$ -CNC NPs, and  $^{177}\text{LuLu}$ -CNC-V NPs in B) murine YUMM1.G1 and human A375 melanoma cell lines at 1, 6, 24, and 48 h of incubation with fixed concentrations of 1 MBq  $\text{mL}^{-1}$  for  $^{177}\text{Lu}$ , 40  $\mu\text{g mL}^{-1}$  for CNC NPs and  $0.1 \times 10^{-6}$  M for vemurafenib. The statistic was analyzed using the unpaired Student's *t*-test between  $^{177}\text{LuLu}$ -CNC NPs and  $^{177}\text{LuLu}$ -CNC-V NPs at the same incubation time point where the significant probabilities were set at n.s. (not significant,  $p > 0.05$ ), \* $p < 0.05$ , \*\* $p < 0.01$ , and \*\*\* $p < 0.001$ . Columns represent the mean  $\pm$  s.d. ( $n = 3$ ).



**Figure 7.** Representative qualitative clonogenic cell survival assay in murine YUMM1.G1 and human A375 melanoma cells regrown after treatments in fresh medium (1), PLL-CNC NPs (2), free vemurafenib (3), free  $[^{177}\text{Lu}]\text{Lu}^{3+}$  (4),  $[^{177}\text{Lu}]\text{Lu}$ -CNC NPs (5), and  $[^{177}\text{Lu}]\text{Lu}$ -CNC-V NPs (6) at doses of 1 MBq mL<sup>-1</sup> for  $^{177}\text{Lu}$ , 40  $\mu\text{g mL}^{-1}$  for CNC NPs, and  $0.1 \times 10^{-6}$  M for vemurafenib at 6, 24, and 48 h.

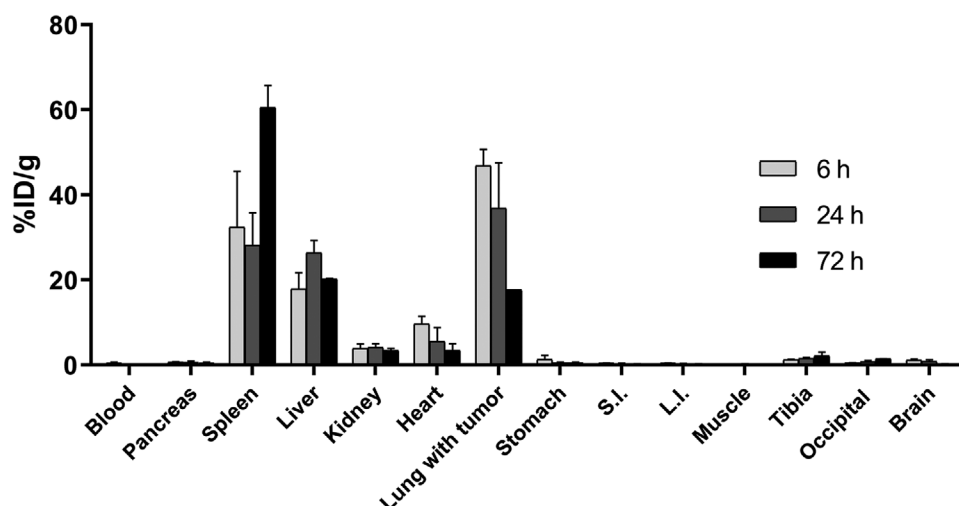
qualitative analysis through the overall intensity of the crystal violet staining in the samples. The theranostic  $[^{177}\text{Lu}]\text{Lu}$ -CNC-V NPs revealed to be the most effective formulation, and there were no cell colonies formed after 24 and 48 h treatments in both cell lines. There was no clear difference in the stained cell colonies between samples treated with non-radioactive components (vemurafenib and PLL-CNC NPs) alone compared to the negative control in all tested cell lines and time points. Undoubtedly, the PLL-CNC NPs are nontoxic and should not cause cytotoxicity, while in contrast vemurafenib at  $0.1 \times 10^{-6}$  M should already exhibit cytotoxic effects after 24 h incubation, as shown by the CellTiter-Glo assay results earlier. The lack of cytotoxic effects observed in the clonogenic assay for these components could be a result of drug resistance behavior in which different complex mechanisms, such as the efflux of anticancer drugs, the escape from therapy-induced senescence, and the enhanced DNA damage repair are elicited in response to treatment. This phenomenon only becomes apparent in the clones grown for the relatively long period of 10 d as opposed to the three day time frame of the cell viability assay.<sup>[47]</sup> The murine YUMM1.G1 cell line appears to be more radiosensitive than the human A375 cell line by comparison of the intensity of the crystal violet staining; however, the mechanisms underlying the differences in intrinsic radiosensitivity of cancer cell lines are variable and still under investigation.<sup>[48]</sup> Nevertheless, our results indicate that there is potential added therapeutic efficacy in the combination of BRAF inhibition with vemurafenib and  $^{177}\text{Lu}$  radiotherapy delivered in a single CNC NP platform in BRAF V600E-mutated melanoma, but with the limitations in the present clonogenic assay the molecular mechanism needs to be investigated in more detail in future studies. Furthermore, our results on the potential added efficacy of the chemoradiotherapeutic combination are in line with those reported by Dasgupta and co-workers<sup>[49]</sup> in vitro with the

combination of PLX4720 (another BRAF V600E targeting inhibitor) and external beam radiotherapy (EBRT). In that case, the potential mechanism underlying the added effects could be the suppression of ionizing radiation-induced MEK/ERK pathway activation by BRAF inhibition.<sup>[50,51]</sup> However, without a doubt the whole picture is more complex and the potential added or synergistic effects of BRAF inhibition and targeted radiotherapy will depend on the relative timing and doses of the two treatment modalities.<sup>[52,53]</sup>

## 2.7. Ex Vivo Biodistribution and Dosimetry

The ex vivo biodistribution of the  $[^{177}\text{Lu}]\text{Lu}$ -CNC-V NPs was first evaluated in YUMM1.G1 lung metastatic melanoma bearing C57BL/6NRj female mice prior to the therapeutic studies as the first step to examine the distribution profiles of the developed theranostic CNC NPs in vivo as a function of time. The YUMM1.G1 cell is a congenic mouse melanoma cell line with C57BL/6J strain background and with defined genotype of *Braf*<sup>V600E/wt</sup> *Pten*<sup>-/-</sup> *Cdkn2*<sup>-/-</sup> *Mc1r*<sup>e/e</sup> developed in the Yale University Mouse Melanoma (YUMM) series.<sup>[54]</sup> The  $[^{177}\text{Lu}]\text{Lu}$ -CNC-V NPs were successfully radiolabeled with  $^{177}\text{Lu}$  (RCY = 64%) and loaded with vemurafenib (%LE = 19%) with a high radiochemical purity (RCP = 98.9%) upon the administration. The final concentrations of CNC NPs, vemurafenib, and  $^{177}\text{Lu}$  were 1 mg kg<sup>-1</sup>, 2 mg kg<sup>-1</sup>, and 1.2 MBq per injection, respectively, formulated in 150  $\mu\text{L}$  of sterilized 1 $\times$  PBS supplemented with 5% Solutol HS 15. As expected, the  $[^{177}\text{Lu}]\text{Lu}$ -CNC-V NPs demonstrated high but transient retention in the lung with average values of 47%ID g<sup>-1</sup> at 6 h, 37%ID g<sup>-1</sup> at 24 h, and 18%ID g<sup>-1</sup> at 72 h (Figure 8), which correspond to our previous report on the behavior of  $[^{111}\text{In}]\text{In}$ -CNC NPs in vivo.<sup>[31]</sup> The transient accumulation is likely a result of the rheology of the needle-like particles in the





**Figure 8.** Ex vivo biodistribution profiles of the radioactivity after the administration of the  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs in YUMM1.G1 lung metastatic melanoma-bearing C57BL/6NRj female mice at 6, 24, and 72 h postinjection. The values represent the mean  $\pm$  s.d. ( $n = 3$ ). %ID  $\text{g}^{-1}$  = percent of injected dose per gram of tissue, S.I. for the small intestine, and L.I. for the large intestine.

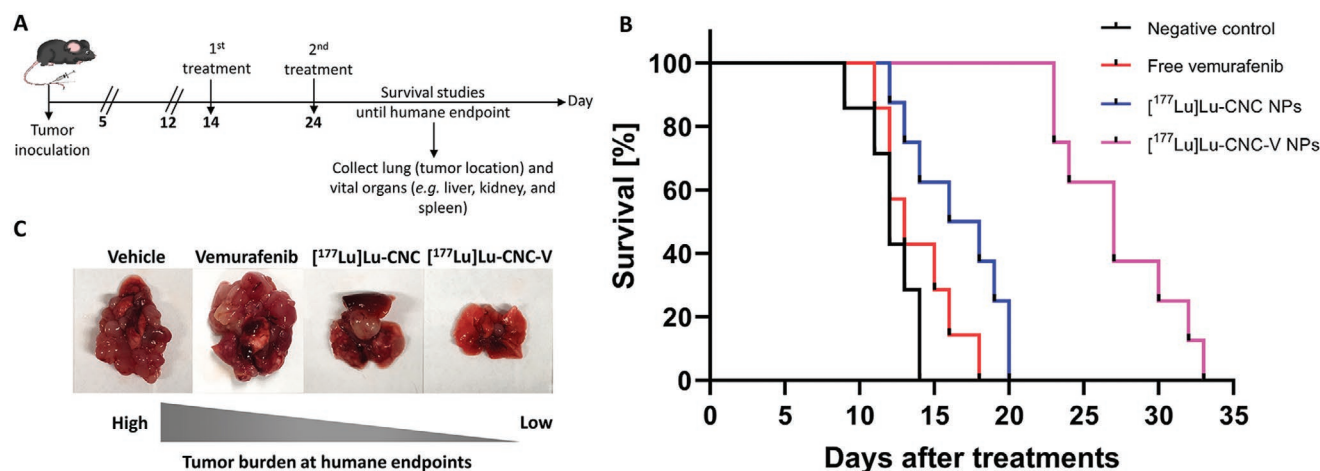
lung vascular bed, as they tend to tumble close to the vessel walls and can potentially embolize in narrow capillaries and tumor neovascularization.<sup>[55,56]</sup> The entrapped  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs in the blood vessels potentially sustain the release of vemurafenib to the metastatic site by passive diffusion through the capillaries, meanwhile the ionizing  $\beta^-$  particles emitted by  $^{177}\text{Lu}$  on the CNC NPs can penetrate and accumulate in metastatic lesions with a maximum penetration range of 2 mm in soft tissues.<sup>[57]</sup> No acute adverse effects of this trapping were seen in the mice as the dispersion stability is properly maintained by the solubilizer in the optimized NP formulation. Major uptake was also seen in the liver (18–26%ID  $\text{g}^{-1}$ ) and spleen (28–60%ID  $\text{g}^{-1}$ ), which are sites for the clearance of nontargeted NPs through the mononuclear phagocyte system (MPS). The values in the kidney (<4%ID  $\text{g}^{-1}$ ) and other excised tissues (<1%ID  $\text{g}^{-1}$ ) revealed no significant accumulation over the period of studies indicating in vivo stability of the construct. Furthermore, there was no acute toxicity or severe side effects noticed during the course of the biodistribution studies. Therefore, the biodistribution profile and animal health status after the treatment suggest the potential use of the  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs for treating melanoma metastases in the lung through the enhanced retention in the lung vascular bed and potentially in the metastasis neovascularization itself.

The results of the ex vivo biodistribution were used to estimate the absorbed dose in select organs, which could be used as a guideline for the safe administration dose of  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs in order to minimize the radiation burden in nontarget organs. The dosimetry calculation showed high total absorbed doses in the lung with tumor (232.38 cGy per MBq), liver (418.33 cGy per MBq), and spleen (1056.03 cGy per MBq) while only low absorbed doses were observed in the kidney (54.26 cGy per MBq), heart (36.42 cGy per MBq) and other tissues (<5 cGy per MBq, Table S5, Supporting Information). There is not much research to date on the dosimetry or radiotoxicity of  $^{177}\text{Lu}$ -radiolabeled nanoparticles in small animal models. However, widely varying doses ranging from 6 to

55.5 MBq of  $^{177}\text{Lu}$ -radiolabeled peptides and antibodies have been used in therapeutic studies for mice,<sup>[58–61]</sup> which could be used as a starting point for the estimation of safe radioactive doses in the treatment plan. Naturally, the clearance patterns and rates for peptides and antibodies are considerably different from nanomaterials, and the role of the spleen as a dose-limiting organ in this experimental setup cannot be overlooked.

## 2.8. Therapeutic Studies

Following the biodistribution study, therapeutic studies were conducted to explore the potential synergistic effects of vemurafenib chemo- and  $^{177}\text{Lu}$  radiotherapy delivered by the theranostic  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs through monitoring of the survival rate of YUMM1.G1 lung metastatic melanoma-bearing animals comparing to the survival in animals treated with the vehicle only (negative control), free vemurafenib (positive control), and the  $[^{177}\text{Lu}]\text{Lu-CNC}$  NPs alone. The  $[^{177}\text{Lu}]\text{Lu-CNC}$  NPs were selected as the single-modality treatment where the therapeutic efficacy is solely generated from the ionizing radiation of  $^{177}\text{Lu}$ , as the biodistribution pattern of free  $[^{177}\text{Lu}]\text{Lu}^{3+}$  would be considerably different and studying the radiometal alone would not be meaningful in terms of tumor accumulation according to the results of the cell uptake assay in YUMM1.G1. After 14 d of tumor inoculation, the first treatment was administered followed by the second round of treatment after 10 d. The animal weight and body condition score were monitored daily after the initiation of the treatment and lung with tumor tissues and vital organs (e.g., liver, kidney, and spleen) were collected to observe the tumor burden and potential metastasis in other organs at the humane endpoint (Figure 9A). The injected  $[^{177}\text{Lu}]\text{Lu-CNC}$  NPs and  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs were prepared at high radiolabeling yield and radiochemical purity. The radiochemical yield, radiochemical purity, drug loading efficiency, and drug loading degree of the  $[^{177}\text{Lu}]\text{Lu-CNC}$  NPs and  $[^{177}\text{Lu}]\text{Lu-CNC-V}$  NPs for both constructs are compiled in Table S6, Supporting



**Figure 9.** A) Timeline of therapeutic studies, B) Kaplan-Meier survival plot as a function of time after treatments with the vehicle (negative control), free vemurafenib,  $[^{177}\text{Lu}]\text{Lu-CNC NPs}$ , and  $[^{177}\text{Lu}]\text{Lu-CNC-V NPs}$  ( $n = 7-8$  per group), where the administered doses of vemurafenib, CNC NPs, and radioactivity were fixed at 3.5, 1.25  $\text{mg kg}^{-1}$ , and 2 MBq per animal per treatment round, respectively. Day 0 on the x-axis indicates as the day of the second treatment. C) Representative images of tumor burden in the lung tissue collected at the humane endpoint of each injected formulation.

Information. The administered doses of  $^{177}\text{Lu}$ , vemurafenib, and CNC NPs were fixed at 2 MBq, 3.5  $\text{mg kg}^{-1}$ , and 1.25  $\text{mg kg}^{-1}$ , respectively, per treatment round. The humane endpoints were set based on the weight loss exceeding the 20% threshold using the weight on the second treatment day as the baseline in combination with the health status of the animals (body condition score of 2 on two consecutive observations, labored breathing, and cyanosis). The Kaplan-Meier survival analysis revealed superior therapeutic effects of the  $[^{177}\text{Lu}]\text{Lu-CNC-V NPs}$  compared to other groups (the Mantel-Cox test,  $p$ -value < 0.0001) after treatments (Figure 9B). The animals treated with the theranostic  $[^{177}\text{Lu}]\text{Lu-CNC-V NPs}$  displayed the longest median survival time of 27 d after treatment followed by cohorts treated with the  $[^{177}\text{Lu}]\text{Lu-CNC NPs}$  (17 days), free vemurafenib (13 d), and vehicle (12 d). There was no acute toxicity observed in any of the treatment groups upon administration. The survival studies demonstrated the evident synergism of vemurafenib chemotherapy and  $^{177}\text{Lu}$  radiotherapy generated from the  $[^{177}\text{Lu}]\text{Lu-CNC-V NPs}$  in pulmonary metastatic melanoma model, which pave the way for the development of CNC-based theranostic nanosystem for combination therapy of metastatic melanoma with improved pharmacokinetics and antitumor efficacy.

Furthermore, the cohort treated with the  $[^{177}\text{Lu}]\text{Lu-CNC-V NPs}$  showed less tumor burden in the lung at the humane endpoint compared to the other treatment groups (Figure 9C). Although the survival of mice treated with the  $[^{177}\text{Lu}]\text{Lu-CNC-V NPs}$  was improved, it could not be further prolonged in this study because of ultimately fatal secondary metastases found in the cardiac muscle (75%, 6/8, Figure S4, Supporting Information) and thoracic cavity (25%, 2/8). These were not discovered in other treatment groups, suggesting that they are not characteristic of the progression of YUMM1.G1 tumors. Further studies into this are warranted, as this is to our knowledge the first account of the use of this cell line in an orthotopic model of lung metastatic melanoma. In general, cardiac metastasis is rarely found at the first instance in intravenous models, which is similar to the observations in this study. This might be a result of the escape of radiation- or vemurafenib-resistant cells

from the original tumor site. There are four possible pathways to the spread of cells to the heart and chest cavity, including direct extension, the bloodstream, the lymphatic system, and intracavitary diffusion through the inferior vena cava or pulmonary veins.<sup>[62]</sup> Among these, the lymphatic system is believed to be the most plausible route since the lung and heart have multiple connective lymph channels that resistant melanoma cells could migrate in, coalesce into the mediastinum and eventually drain to the thoracic duct.<sup>[63]</sup> Future efforts should be targeted to resolving this issue with the DDS, potentially by increasing the radioactive or pharmaceutical doses or adjusting the timing and frequency of the therapeutic administration which fell beyond the scope of this study. Also, studies with less aggressive human BRAF V600E-positive A375 xenografts or patient-derived xenografts are warranted.

Histological examination of the H&E sections of select vital organs after treatment with all formulations revealed normal architecture with no sign of radiation burden or secondary metastasis compared to the vehicle control group (Figure S5, Supporting Information). This indicated no severe radiotoxicity in liver and spleen tissues after two consecutive treatments and suggested safety of the theranostic formulation. However, the immunohistochemical Ki-67 staining of the lung infiltrated tumor at the humane endpoints showed no significant difference in cell proliferation markers in all treatment groups (Figure S5, Supporting Information). This is likely because the animals from each group were euthanized upon meeting the criteria for a humane endpoint, at a minimum of 12 d after the second treatment (vehicle group) or considerably later, not at a fixed time point after the treatment. As a consequence, differences in the impact of the treatments on the proliferative capacity of the tumor cells could not be detected. These effects between the treatment groups could have been more evident closer to the time of theranostic nanosystem administration. Furthermore, in patients, BRAF kinase inhibition has been shown to elicit severe adverse effects if not discontinued during EBRT,<sup>[64]</sup> which were not seen in this study with local radiotherapy. Therefore, it seems that the radiosensitizing effect of

vemurafenib could be harnessed to potentiate the effects of the radiotherapy in this previously unexplored strategy to the treatment of pulmonary metastasis of melanoma.

In summary, the therapeutic study results confirm that the transient trapping of the theranostic CNC NP-based DDS in the lung is a viable strategy for therapeutic delivery to the lung and to pulmonary metastases, alluding to potential clinical utility of CNC-based DDS after systemic administration, which has remained challenging with CNC-based biomaterials to date.

### 3. Conclusion

Taken together, the [ $^{177}\text{Lu}$ ]Lu-CNC-V NPs developed in this work demonstrate the feasibility of using CNC NPs as a naturally sourced and renewable nanoscale platform for theranostic nanosystems for the treatment of BRAF V600E positive metastatic melanoma in the lung with radiotherapy and kinase inhibition after systemic delivery. The energy and tissue range of  $\beta^-$  particles emitted by  $^{177}\text{Lu}$  as well as the rate of the sustained release of the vemurafenib were appropriate for the application, resulting in the prolonged survival of YUMM1.G1 tumor-bearing mice receiving the theranostic combination. The system is modular, as the trivalent radiometal, the capping agent, and drug payload can be exchanged to generate new theranostic combinations and tailor the properties of the DDS. Furthermore, future efforts should be dedicated to elucidating the mechanism of the transient trapping of the CNC NPs in the lung and the possibility of modulating this behavior through CNC NP engineering to enhance delivery to lung tissue and pulmonary metastases.

### 4. Experimental Section

**Materials and Chemicals:** All general chemicals and anhydrous organic solvents as well as human serum were purchased from Merck (St. Louis, MO, USA) unless otherwise denoted and used without additional purification. Cotton fiber derived CNC NPs were prepared from ashless Whatman filter paper through acid hydrolysis as described in literature<sup>[65,66]</sup> and the acid residue was washed out with excess amount of dimethyl sulfoxide (DMSO) and ultrapure water before further syntheses. The 1,4,7,10-tetraazacyclododecane-1,4,7-tris(acetic acid)-10-(4-aminobutyl) acetamide (DOTA-amine or DOTA-NH<sub>2</sub>) was acquired from Macrocyclics (Plano, TX, U.S.A.). Vemurafenib (purity > 98%) was obtained from Adooq Bioscience (Irvine, CA, USA). Poly-L-lysine hydrochloride or PLL (MW 1.6 kDa with 10 repeating units of L-lysine) was purchased from Alamanda Polymers (Huntsville, AL, USA). The dialysis membrane (MWCO 12–14 kDa) was obtained from Spectrum Laboratories (Waltham, MA, USA). [ $^{177}\text{Lu}$ ]LuCl<sub>3</sub> was acquired from Curium Pharma (Petten, The Netherlands). The polypropylene protein LoBind microcentrifuge tubes (1.5 mL) were obtained from Eppendorf (Hamburg, Germany). The Solutol HS 15 solubilizer was acquired from BASF ChemTrade GmbH (Burgbernheim, Germany). The glass microfiber chromatography sheets impregnated with silicic acid (iTLC-SA) were acquired from Agilent Technologies (Folsom, CA, USA). Donor human plasma (FFP 24) was obtained from the Finnish Red Cross Blood Service (Helsinki, Finland) under an ethical approval for research purposes. Ultrapure water (18.2 M $\Omega$  cm at 25 °C, 2 ppb TOC) was prepared in-house by a Milli-Q Integral 10 water purification unit equipped with 0.22  $\mu\text{m}$  Millipak Express 40 membrane filter (Merck Millipore, Burlington, MA, USA) at the point of dispense for producing bacteria- and particulate-free ultrapure water. Cell culture reagents and general procedures are described in the Supporting Information.

**Preparation of DOTA-Modified CNC NPs:** The bifunctional DOTA chelator-functionalized CNC (DOTA-CNC) NPs used in this work were synthesized by the conjugation of DOTA-amine to the hydroxyl groups on the surface of the CNC NPs as previously reported.<sup>[31]</sup> Briefly, the CNC NPs were dispersed in anhydrous DMSO at a concentration of 5 mg mL<sup>-1</sup> and sonicated for 5 min at 20% amplitude tip sonicator (QSonica, Newton, CT, USA). Carbonyldiimidazole (CDI, 2 eq w/w) in anhydrous DMSO was added to the CNC solution while flushing with argon flow and constant agitation. The reaction was left stirring overnight in a temperature-controlled silicone oil bath at 60 °C under argon atmosphere. The unreacted CDI was washed out twice with 5 mL of fresh DMSO and the CDI-activated CNC NPs were collected by centrifugation at 4000 rpm for 5 min (Heraeus Megafuge 1.0R, Thermo Fisher Scientific, Waltham, MA, USA). The CDI-activated CNC NPs were redispersed in anhydrous DMSO (5 mg mL<sup>-1</sup>) and the solution was constantly flushed with argon flow for 10 min while stirring. Then, the DOTA-amine (1 eq w/w) in anhydrous DMSO was added dropwise to the CDI-activated CNC solution. The reaction was continued for 3 d under argon atmosphere at 60 °C, meanwhile, the argon balloon was refilled daily to maintain a sufficient inert atmosphere inside the reaction flask. Following the 3-day reaction, the mixture was centrifuged and the collected DOTA-CNC NPs were washed twice with 5 mL of fresh DMSO to remove any unreacted DOTA-amine. The DOTA-CNC NPs were further dialyzed against ultrapure water for 3 d with at least four changes of water daily. Finally, the DOTA-CNC NPs were collected by centrifugation and lyophilized.

**Material Characterization:** The elemental composition of unmodified and modified CNC NPs was analyzed using a Vario MICRO Cube CHNS analyzer (Elementar Analysensysteme GmbH, Lagensfeld, Germany) and are reported as a percent of carbon (C), hydrogen (H), and nitrogen (N). The CNC NPs were further characterized with a Spectrum One Fourier transform infrared spectrometer (FTIR) equipped with an attenuated total reflectance (ATR) unit (PerkinElmer Instruments LLC, Shelton, CT, USA). The electrokinetic potential of unmodified and modified CNC NPs in ultrapure water ( $\zeta$ -potential) was measured using a Zetasizer Nano ZS instrument (Malvern, Worcestershire, UK) at a concentration of 300  $\mu\text{g mL}^{-1}$ . The morphology and dimensions (width and length) of CNC NPs were determined with a Hitachi S-4800 field emission-scanning electron microscope at 10 kV (FE-SEM, Hitachi, Tokyo, Japan). The FE-SEM samples were prepared by dispersing the CNC NPs in ultrapure water at a concentration of 25  $\mu\text{g mL}^{-1}$  and sonicated for 2 min. The silicon wafer substrates were taped to the cylindrical specimen holder and wiped with ultrapure water followed by blowing with the compressed air to remove dust from the surface. Then, an aliquot of CNC samples (10  $\mu\text{L}$ ) was applied on the silicon wafer and left to dry in a desiccator overnight. The same procedure was repeated once on each substrate in order to get an adequate number of particles for the imaging. Prior to imaging, the samples were coated with a 3 nm layer of Au-Pd alloy in a high-resolution sputtering coater (208HR, Cressington Scientific Instruments, Watford, UK) in order to increase the conductivity and signal-to-noise ratio of the samples. The dimensions (width and length) of each sample ( $n \geq 100$  particles) were determined from the images using ImageJ 1.52i software.

**Radiolabeling of DOTA-CNC NPs:** Before radiolabeling experiments, ultrapure water used for the preparation of all radiolabeling buffer solutions was pretreated with Chelex 100 ion-exchange resin (Bio-Rad, Hercules, CA, USA) at a concentration of 5 g L<sup>-1</sup> for 24 h and filtered through a 0.22  $\mu\text{m}$  membrane to obtain the metal-free water. The DOTA-CNC NPs (1 mg mL<sup>-1</sup>) were dispersed in 0.2 M ammonium acetate buffer (pH 4.0) in a 1.5 mL Protein LoBind microcentrifuge tube (Eppendorf, Hamburg, Germany). The DOTA-CNC solution was sonicated for 5 min at 20% amplitude on a tip sonicator. [ $^{177}\text{Lu}$ ]LuCl<sub>3</sub> (20–180 MBq) was added to the DOTA-CNC solution. The radiolabeling reaction was heated to 100 °C in a digital dry bath heater (AccuBlock, Labnet International, Edison, NJ, USA) placed on an orbital shaker at 600 rpm for 1 h. Following the incubation, the reaction mixture was equilibrated to room temperature and quenched with 100  $\mu\text{L}$  of 50  $\times$  10<sup>-3</sup> M DTPA solution. The reaction vial was centrifuged at 10 000 g for

5 min to collect the  $^{177}\text{Lu}$ -Lu-CNC pellet. The supernatant was removed, and the product pellet was purified with sequential washes in  $50 \times 10^{-3}$  M DTPA solution twice, three times with  $1\times$  PBS (pH 7.4), and once with metal-free ultrapure water with a collection of the radiolabeled CNC NPs by centrifugation after each step. The radioactivity in both supernatant and the collected pellet was monitored using a VDC-603 dose calibrator (VIK-202 ionization chamber model, Comcer, Joure, The Netherlands) after every step. Then, the purified radiolabeled product was redispersed in  $1\times$  PBS (pH 7.4) and the quality control was done by radio-TLC. An aliquot of radiolabeled CNC solution ( $1\text{--}2\ \mu\text{L}$ ) was spotted on the iTLC-SA chromatography sheet and run in a closed glass chamber with  $0.1\ \text{M}$  citrate buffer (pH 5.0). The  $^{177}\text{Lu}$ -Lu-CNC NPs remain at the baseline of the application spot ( $R_f = 0$ ) while the free  $^{177}\text{Lu}$ -Lu $^{3+}$  moves along with the solvent front ( $R_f = 0.9\text{--}1.0$ ). After air-drying, the iTLC-SA sheet was exposed to a digital imaging plate for photostimulated luminescence (PSL) detection (Fuji BAS-TR2025,  $20 \times 25\ \text{cm}$ ) for 2 min. The imaging plate was scanned on a Fujifilm Fluorescent Image Analyzer (FLA-5100 V.1, Fuji Film Photo, Tokyo, Japan). The radiochemical purity (RCP) of the  $^{177}\text{Lu}$ -Lu-CNC NPs was analyzed using AIDA image analysis software version 5.0 SP 3 (Elysia-Raytest GmbH, Straubenhardt, Germany).

**Radiolabel Stability and EDTA/ $\text{Fe}^{3+}$  Challenges:** The in vitro radiolabel stability of the  $^{177}\text{Lu}$ -Lu-CNC NPs was evaluated in simulated physiological conditions, including  $1\times$  PBS (pH 7.4), and 50 and 100% human plasma, and in the presence of competing for  $0.2 \times 10^{-3}$  M  $\text{FeCl}_3$  and  $2 \times 10^{-3}$  M EDTA. The  $^{177}\text{Lu}$ -Lu-CNC NPs were dispersed in the specified buffer at a concentration of  $100\ \mu\text{g mL}^{-1}$  and incubated at  $37\ ^\circ\text{C}$  at 500 rpm. Samples ( $2\ \mu\text{L}$ ) were drawn and spotted on the iTLC-SA chromatography paper at specified time points (1, 2, 4, 6, 16, 24, 48, 72, and 96 h). The radio-TLC chromatograms were run in  $0.1\ \text{M}$  citrate buffer (pH 5.0) and the percentage of  $^{177}\text{Lu}$  remaining on the surface of the CNC NPs was quantified using digital autoradiography as described in the previous section. All assays were carried out in triplicate.

**Drug Loading:** The drug loading of both nonradiolabeled and radiolabeled CNC NPs was carried out in a one-pot reaction. Either unmodified CNC NPs or  $^{177}\text{Lu}$ -Lu-CNC NPs ( $1\ \text{mg}$ ) were dispersed in  $200\ \mu\text{L}$  of anhydrous DMSO in a  $1.5\ \text{mL}$  Protein LoBind microcentrifuge tube. Vemurafenib ( $1:1\ \text{w/w}$ ) and PLL ( $1:10\ \text{w/w}$ ) in anhydrous DMSO were added to the CNC dispersion. The reaction volume was adjusted with fresh anhydrous DMSO to a total solid concentration of  $6\ \text{mg mL}^{-1}$ . The reaction mixture was sonicated for 2 min at 30% amplitude and further incubated at  $37\ ^\circ\text{C}$  for 1 h on a shaker at 750 rpm (Eppendorf Thermomixer C, Eppendorf, Hamburg, Germany). The reaction vial was centrifuged at  $10\ 000\ \text{g}$  for 10 min. The supernatant was removed and filtered through a  $0.2\ \mu\text{m}$  PVDF  $13\ \text{mm}$  diameter filter (Acrodisc, Pall Corporation, Port Washington, NY, USA). The amount of vemurafenib in the supernatant (unbound drug) was quantified using high-performance liquid chromatography (Prominence HPLC system, Shimadzu Corporation, Kyoto, Japan). The separations were carried out on a reverse-phase XBridge  $\text{C}_{18}$  analytical column ( $130\ \text{\AA}$ ,  $5\ \mu\text{m}$ ,  $4.6 \times 250\ \text{mm}$ , Waters Corporation, Milford, MA, USA) with an isocratic flow of  $0.1\ \text{M}$  glycine buffer (pH 9.0) and acetonitrile (45:55) eluent system at a flow rate of  $0.9\ \text{mL min}^{-1}$ , and  $254\ \text{nm}$  UV detection. The retention time of vemurafenib was  $8.70\text{--}8.79\ \text{min}$ . The amount of vemurafenib was quantified using a vemurafenib standard curve ranging from  $1.56$  to  $200\ \mu\text{g mL}^{-1}$  ( $R^2 = 1$ ). The drug loading efficiency (%LE) and loading degree (%LD) were determined using equations detailed in the Supporting Information. All samples were analyzed in triplicate.

**In Vitro Drug Release Profiles:** The in vitro drug release experiments were conducted in  $1\times$  PBS buffer (pH 7.4) and tumor microenvironment mimicking conditions ( $10 \times 10^{-3}$  M acetate buffer pH 5.5, representing the late endosome).<sup>[67]</sup> Both buffer systems were supplemented with 10% (v/v) human serum to induce sink conditions for drug dissolution. The nonradiolabeled PLL-CNC-V NPs and  $^{177}\text{Lu}$ -Lu-CNC-V NPs containing  $200\ \mu\text{g}$  of CNC NPs and  $22\ \mu\text{g}$  of vemurafenib were dispersed in  $500\ \mu\text{L}$  of the respective buffers in Protein LoBind microcentrifuge tubes and incubated at  $37\ ^\circ\text{C}$  with 500 rpm shaking. At each time point (1, 2, 4, 6, 12, 24, 48, 72, and 96 h), sample vials were centrifuged at 5000 rpm

for 10 min and the supernatant was collected to a new microcentrifuge tube. The sample pellets were redispersed with an equal initial volume ( $500\ \mu\text{L}$ ) of corresponding media and the incubation was continued. Proteins in the isolated supernatant were denatured by adding an ice-cold acetonitrile ( $1:1\ \text{v/v}$ ) and pelleted by centrifugation at  $9\ 000\ \text{g}$  for 10 min. The protein precipitates were discarded, and the collected supernatants were lyophilized overnight. The lyophilized samples were dissolved in  $500\ \mu\text{L}$  of HPLC grade DMSO and passed through  $0.2\ \mu\text{m}$  PVDF filter before HPLC analysis. The amount of released vemurafenib was quantified using the HPLC method described previously. All samples were analyzed in triplicate.

**In Vitro Cell Viability Studies:** The in vitro cytotoxicity was determined using a commercial CellTiter-Glo luminescent cell viability assay, which is the most appropriate assay for the CNC NPs according to previous reports.<sup>[31,32]</sup> Murine YUMM1.G1 and human A375 cell lines were chosen as mouse and human melanoma cell models harboring the activating BRAF V600E mutation while murine B16-F10 skin melanoma cell expressing wild-type BRAF gene was used as the negative control cell line. Cells were plated at a density of 5000 cells per well on an opaque-walled 96-well plate with clear bottom in  $100\ \mu\text{L}$  of the corresponding media and allowed to attach overnight. The media was removed and replaced with  $100\ \mu\text{L}$  of the corresponding media containing free vemurafenib, PLL-CNC NPs (empty particle), or PLL-CNC-V NPs at drug concentration of  $0.1 \times 10^{-6}$ ,  $0.5 \times 10^{-6}$ ,  $1.0 \times 10^{-6}$ , and  $1.5 \times 10^{-6}\ \text{M}$ . The PLL-CNC NP concentrations were determined in correspond with the amount of the CNC NPs used in the PLL-CNC-V formulation:  $0.5$ ,  $2.2$ ,  $4.5$ , and  $6.7\ \mu\text{g mL}^{-1}$  for  $0.1 \times 10^{-6}$ ,  $0.5 \times 10^{-6}$ ,  $1.0 \times 10^{-6}$ , and  $1.5 \times 10^{-6}\ \text{M}$ , respectively. Fresh medium and Triton X-100 solution ( $1\% \text{ v/v}$ ) were used as negative and positive controls for cytotoxicity, respectively. The plates were incubated at  $37\ ^\circ\text{C}$ ,  $5\% \text{ CO}_2$  atmosphere and  $95\%$  relative humidity for 6, 24, 48, and 72 h. Moreover, to corroborate the sensitivity of the cell lines to vemurafenib, western blot analysis was carried out to observe the decrease in phosphorylation of mitogen-activated protein kinase kinase (MEK, the downstream target of BRAF) in response to vemurafenib at  $0.1 \times 10^{-6}$  and  $1 \times 10^{-6}\ \text{M}$  concentration for 6, 24, and 48 h. The protocols for cytotoxicity determination and western blot analysis are detailed in the Supporting Information.

**Cellular Uptake Studies of Radiolabeled CNC Constructs:** The in vitro cell internalization of radiolabeled CNC constructs was studied in YUMM1.G1 and A375 melanoma cell lines. Cells were seeded on a transparent 12-well plate at a density of 25 000 cells per well and allowed to attach overnight. Prior to the experiments, the cells were acclimatized to the  $\text{CO}_2$  independent medium supplemented with  $10\%$  FBS and  $1\%$  penicillin–streptomycin at  $37\ ^\circ\text{C}$  incubator with  $0\% \text{ CO}_2$  for at least 30 min. The medium was removed and replaced with  $1\ \text{mL}$  of  $\text{CO}_2$  independent medium containing free  $^{177}\text{Lu}$ -Lu $\text{Cl}_3^{3+}$ ,  $^{177}\text{Lu}$ -Lu-CNC NPs, or  $^{177}\text{Lu}$ -Lu-CNC-V NPs. The radioactivity of  $^{177}\text{Lu}$  in each sample was set at  $1\ \text{MBq mL}^{-1}$  while the CNC NPs and vemurafenib doses were  $40\ \mu\text{g mL}^{-1}$  and  $0.1 \times 10^{-6}\ \text{M}$ , respectively. Cells were incubated at  $37\ ^\circ\text{C}$  for 1, 6, 24, and 48 h. At each time point, the cells were treated to yield fractions for unbound, membrane-bound and internalized radioactivity. Details for the uptake protocol are described in the Supporting Information.

**Clonogenic Assay:** The in vitro clonogenic cell survival was evaluated in murine YUMM1.G1 and human A375 melanoma cell lines. Both cell lines were treated with non-radiolabeled PLL-CNC NPs, free vemurafenib, free  $^{177}\text{Lu}$ -Lu $\text{Cl}_3^{3+}$ ,  $^{177}\text{Lu}$ -Lu-CNC NPs, and  $^{177}\text{Lu}$ -Lu-CNC-V NPs while the untreated cells (negative control for cytotoxicity) were incubated with  $\text{CO}_2$  independent medium throughout the study. The concentrations of radioactivity, CNC NPs, and vemurafenib were fixed at  $1\ \text{MBq mL}^{-1}$ ,  $40\ \mu\text{g mL}^{-1}$ , and  $0.1 \times 10^{-6}\ \text{M}$ , respectively. At the specified time points (6, 24, and 48 h), the cells were collected and cultured for further 10 d in fresh medium on six-well plates. At the end of the assay period, the cell colonies were stained with crystal violet and the plates were scanned for colony observation. The experimental procedure is described in the Supporting Information.

**Ex Vivo Biodistribution, Dosimetry, and Therapeutic Studies:** All animal experiments in this work were conducted under a project license number ESAVI/12132/04.10.07/2017 approved by the National Board of Animal



Experimentation in Finland and in compliance with the European Union Directive 2010/63/EU. In general, animals were group-housed in conventional polysulfones cages supplied with aspen bedding, nesting material (Tapvei, Harjumaa, Estonia) and enrichment (aspen blocks and disposable cardboard hut). Pelleted food (Teklad 2019C diet, Envigo, Huntingdon, UK) and tap water were provided ad libitum. The environmental conditions of the animal housing unit were maintained at 12:12 h light/dark cycle,  $22 \pm 1$  °C, and  $55 \pm 15\%$  relative humidity throughout the experimental period. Both ex vivo biodistribution and therapeutic studies were carried out in YUMM1.G1 lung metastatic melanoma-bearing C57BL/6NRJ mice (female, weighing 16–19 g, aged 8–12 weeks, Janvier Laboratories, Le Genest-Saint-Isle, France). For the orthotopic model of YUMM1.G1 metastatic melanoma in the lung,  $1 \times 10^6$  YUMM1.G1 cells (viability > 95%) in 150  $\mu$ L sterilized 1 $\times$  HBSS were intravenously injected via the lateral tail vein to conscious mice. The tumors were allowed to develop for at least 14 d before the start of the nanotheranostic studies. The summary of injected doses of nanosystem components for biodistribution and therapeutic studies is compiled in Table S7 (Supporting Information).

For ex vivo biodistribution, the [ $^{177}\text{Lu}$ ]Lu-CNC-V NPs were intravenously injected via the tail vein at a dose of 1.2 MBq of [ $^{177}\text{Lu}$ ], 1 mg kg $^{-1}$  of CNC NPs, and 2 mg kg $^{-1}$  of vemurafenib in 150  $\mu$ L of sterilized 1 $\times$  PBS (pH 7.4) supplemented with 5% (v/v) Solutol HS 15. At predetermined time points (6, 24, and 72 h), mice were sacrificed by CO $_2$  asphyxiation followed by cervical dislocation to harvest interest tissue samples, including blood, pancreas, spleen, stomach, liver, kidney, lung with tumor, heart, small intestine, large intestine, skeletal muscle, tibia, occipital bone, and brain. The tissue samples were individually collected and weighted in the 5 mL liquid scintillation tubes. The radioactivity in tissue samples was counted using an automatic gamma counter 1480 Wizard 3". The results were expressed as a percent of injected dose per weight of tissue (%ID g $^{-1}$ ). The number of animals was set at  $n = 3$  per each time point.

Following the ex vivo biodistribution study, the average activity concentration of 2–3 tissue specimens from each time point was fitted to a biexponential function to create a time-activity curve (TAC). For most tissues, the best TAC fit is composed of a one- or two-phase exponential decay model. Notably, the spleen exhibited marked uptake over the measured time course, therefore, a trapezoidal model was used for this tissue up to the latest time point, after which it was assumed that clearance was determined entirely by radioactive decay. The cumulative uptake was calculated from the area under the uptake curves. The absorbed dose to all organs was estimated based on the assumption that the absorbed fraction is equal to 1 for  $\beta^-$  emission of [ $^{177}\text{Lu}$ ] and 0 for the penetrating photon emission with the equilibrium absorbed dose constant of 0.085 Gy/MBq·h (0.31 g·cGy/ $\mu$ Ci·h). The estimated absorbed dose (cGy/MBq) in an individual organ was used as a guideline for the administration plan of safe and effective radiation dose in therapeutic studies to minimize the radiation burden in healthy tissues after the nanotheranostic construct administration.

In therapeutic studies, the animals were randomized into four groups after 14 d of the YUMM1.G1 tumor inoculation: vehicle (1 $\times$  PBS with 6% Solutol HS 15), free vemurafenib (3.5 mg kg $^{-1}$ ), [ $^{177}\text{Lu}$ ]Lu-CNC NPs, and [ $^{177}\text{Lu}$ ]Lu-CNC-V NPs ( $n = 7$ –8 per group). The [ $^{177}\text{Lu}$ ]Lu-CNC and [ $^{177}\text{Lu}$ ]Lu-CNC-V groups were treated with the corresponding theranostic CNC formulations containing 2 MBq of [ $^{177}\text{Lu}$ ], 1.25 mg kg $^{-1}$  of CNC NPs, and 3.5 mg kg $^{-1}$  of vemurafenib per treatment cycle. The second treatment for all groups was done 10 d after the first treatment. The animal weight and condition using body condition scoring<sup>[68]</sup> were monitored and recorded daily until the humane endpoint. At the endpoint, the lung tissue with the tumor and select vital organs (liver, spleen, and kidney) were collected in 10% (v/v) neutral buffered formalin and sent to histological analysis with hematoxylin and eosin (H&E) staining and immunohistochemistry for proliferation using the Ki-67 marker. Details for the immunohistochemical procedure are given in the Supporting Information.

**Statistical Analysis:** Quantitative data are presented as mean  $\pm$  s.d. ( $n \geq 3$ ). A direct comparison between sample groups was made using

unpaired Student's *t*-tests where the statistical significance (*p*-value) was set at  $*p < 0.05$ ,  $**p < 0.01$ , and  $***p < 0.001$ . The survival in therapeutic studies was determined using Kaplan-Meier survival analysis with GraphPad Prism software version 8.0.1 (San Diego, CA, USA).

## Supporting Information

Supporting Information is available from the Wiley Online Library or from the author.

## Acknowledgements

Financial support from the Finnish Cultural Foundation (grant no. 00190375), the Academy of Finland (decision nos. 318422, 278056, 298481, 302102, and 331659), and the University of Helsinki Research Funds are gratefully acknowledged. Finnish Center for Laboratory Animal Pathology (FCLAP) at HiLIFE, University of Helsinki, is acknowledged for the tissue preparation and staining services. The authors also thank Dr. Jaakko Sarparanta for help with phospho-MEK western blot, Ms. Karina Moslova for assistance with the elemental analysis, Ms. Alexandra Correia for assistance with cell culture, and Ms. Petcharada Imlimthan for the assistance with the images.

## Conflict of Interest

The authors declare no conflict of interest.

## Data Availability Statement

The data that support the findings of this study are available from the corresponding author upon reasonable request.

## Keywords

cellulose nanocrystal, drug delivery system, Lutetium-177, metastatic melanoma, theranostic nanosystem, vemurafenib

Received: December 7, 2020

Revised: January 21, 2021

Published online:

- [1] G. C. Leonardi, L. Falzone, R. Salemi, A. Zanghi, D. A. Spandidos, J. A. McCubrey, S. Candido, M. Libra, *Int. J. Oncol.* **2018**, 52, 1071.
- [2] L. E. Davis, S. C. Shalin, A. J. Tackett, *Cancer Biol. Ther.* **2019**, 20, 1366.
- [3] E. Maverakis, L. A. Cornelius, G. M. Bowen, T. Phan, F. B. Patel, S. Fitzmaurice, Y. He, B. Burrall, C. Duong, A. M. Kloxin, H. Sultani, R. Wilken, S. R. Martinez, F. Patel, *Acta Derm.-Venereol.* **2015**, 95, 516.
- [4] E. Erdei, S. M. Torres, *Expert Rev. Anticancer Ther.* **2010**, 10, 1811.
- [5] J. Massague, A. C. Obenauf, *Nature* **2016**, 529, 298.
- [6] M. Holderfield, M. M. Deuker, F. McCormick, M. McMahon, *Nat. Rev. Cancer* **2014**, 14, 455.
- [7] A. Bottos, M. Martini, F. Di Nicolantonio, V. Comunanza, F. Maione, A. Minassi, G. Appendino, F. Bussolino, A. Bardelli, *Proc. Natl. Acad. Sci. USA* **2012**, 109, E353.
- [8] M. Griffin, D. Scotto, D. H. Josephs, S. Mele, S. Crescioli, H. J. Bax, G. Pellizzari, M. D. Wynne, M. Nakamura, R. M. Hoffmann,

- K. M. Ilieva, A. Cheung, J. F. Spicer, S. Papa, K. E. Lacy, S. N. Karagiannis, *Oncotarget* **2017**, *8*, 78174.
- [9] L. Cheng, A. Lopez-Beltran, F. Massari, G. T. MacLennan, R. Montironi, *Mod. Pathol.* **2018**, *31*, 24.
- [10] Z. Yao, R. Yaeger, V. S. Rodrik-Outmezguine, A. Tao, N. M. Torres, M. T. Chang, M. Drosten, H. Zhao, F. Cecchi, T. Hembrough, J. Michels, H. Baumert, L. Miles, N. M. Campbell, E. de Stanchina, D. B. Solit, M. Barbacid, B. S. Taylor, N. Rosen, *Nature* **2017**, *548*, 234.
- [11] M. Dankner, A. A. N. Rose, S. Rajkumar, P. M. Siegel, I. R. Watson, *Oncogene* **2018**, *37*, 3183.
- [12] M. Shinozaki, A. Fujimoto, D. L. Morton, D. S. Hoon, *Clin. Cancer Res.* **2004**, *10*, 1753.
- [13] M. Lidsky, G. Antoun, P. Speicher, B. Adams, R. Turley, C. Augustine, D. Tyler, F. Ali-Osman, *J. Biol. Chem.* **2014**, *289*, 27714.
- [14] A. Saei, P. J. A. Eichhorn, *Cancers* **2019**, *11*, 1176.
- [15] J. L. Manzano, L. Layos, C. Buges, M. de Los Llanos Gil, L. Vila, E. Martinez-Balibrea, A. Martinez-Cardus, *Ann. Transl. Med.* **2016**, *4*, 237.
- [16] S. A. Luebker, S. A. Koepsell, *Front. Oncol.* **2019**, *9*, 268.
- [17] X. Y. Chan, A. Singh, N. Osman, T. J. Piva, *Int. J. Mol. Sci.* **2017**, *18*, 1527.
- [18] T. Langbein, W. A. Weber, M. Eiber, *J. Nucl. Med.* **2019**, *60*, 13S.
- [19] K. J. Yong, D. E. Milenic, K. E. Baidoo, M. W. Brechbiel, *Int. J. Mol. Sci.* **2016**, *17*, 736.
- [20] E. Azorin-Vega, L. Aranda-Lara, E. Torres-Garcia, J. A. Santiago-Banuelos, *Appl. Radiat. Isot.* **2019**, *146*, 24.
- [21] F. U. Din, W. Aman, I. Ullah, O. S. Qureshi, O. Mustapha, S. Shafique, A. Zeb, *Int. J. Nanomed.* **2017**, *12*, 7291.
- [22] S. P. Eguisaguire, M. Igartua, R. M. Hernandez, J. L. Pedraz, *Clin. Transl. Oncol.* **2012**, *14*, 83.
- [23] E. Cukierman, D. R. Khan, *Biochem. Pharmacol.* **2010**, *80*, 762.
- [24] S. Senapati, A. K. Mahanta, S. Kumar, P. Maiti, *Signal Transduction Targeted Ther.* **2018**, *3*, 7.
- [25] Y. Xin, M. Yin, L. Zhao, F. Meng, L. Luo, *Cancer Biol. Med.* **2017**, *14*, 228.
- [26] D. Klemm, B. Heublein, H. P. Fink, A. Bohn, *Angew. Chem., Int. Ed. Engl.* **2005**, *44*, 3358.
- [27] I. Reiniati, A. N. Hrymak, A. Margaritis, *Crit. Rev. Biotechnol.* **2017**, *37*, 510.
- [28] D. Bondeson, A. Mathew, K. Oksman, *Cellulose* **2006**, *13*, 171.
- [29] S. Beck-Candanedo, M. Roman, D. G. Gray, *Biomacromolecules* **2005**, *6*, 1048.
- [30] K. Heise, G. Delepierre, A. W. T. King, M. A. Kostianen, J. Zoppe, C. Weder, E. Kontturi, *Angew. Chem., Int. Ed. Engl.* **2021**, *60*, 66.
- [31] S. Imlimthan, S. Otaru, O. Keinanen, A. Correia, K. Lintinen, H. A. Santos, A. J. Airaksinen, M. A. Kostianen, M. Sarparanta, *Biomacromolecules* **2019**, *20*, 674.
- [32] S. Imlimthan, A. Correia, P. Figueiredo, K. Lintinen, V. Balasubramanian, A. J. Airaksinen, M. A. Kostianen, H. A. Santos, M. Sarparanta, *J. Biomed. Mater. Res., Part A* **2020**, *108*, 770.
- [33] K. J. De France, K. J. Chan, E. D. Cranston, T. Hoare, *Biomacromolecules* **2016**, *17*, 649.
- [34] R. Sunasee, U. D. Hemraz, K. Kless, *Expert Opin. Drug Delivery* **2016**, *13*, 1243.
- [35] M. Sarparanta, J. Pourat, K. E. Carnazza, J. Tang, N. Paknejad, T. Reiner, M. A. Kostianen, J. S. Lewis, *Nucl. Med. Biol.* **2020**, *80–81*, 1.
- [36] X. Tong, Z. Wang, X. Sun, J. Song, O. Jacobson, G. Niu, D. O. Kiesewetter, X. Chen, *Theranostics* **2016**, *6*, 2039.
- [37] S. Eyley, W. Thielemans, *Nanoscale* **2014**, *6*, 7764.
- [38] C. C. Fleischer, C. K. Payne, *J. Phys. Chem. B* **2012**, *116*, 8901.
- [39] A. Albanese, P. S. Tang, W. C. Chan, *Annu. Rev. Biomed. Eng.* **2012**, *14*, 1.
- [40] T. Ganz, E. Nemeth, *Biochim. Biophys. Acta* **2006**, *1763*, 690.
- [41] Letchford, Jackson, B. Wasserman, Ye, W. Hamad, H. Burt, *Int. J. Nanomed.* **2011**, *2011*, 321.
- [42] S. P. Akhlaghi, R. C. Berry, K. C. Tam, *Cellulose* **2013**, *20*, 1747.
- [43] A. M. Barbosa, E. Robles, J. S. Ribeiro, R. G. Lund, N. L. V. Carreno, J. Labidi, *Materials* **2016**, *9*, 1002.
- [44] S. Behzadi, V. Serpooshan, W. Tao, M. A. Hamaly, M. Y. Alkawareek, E. C. Dreaden, D. Brown, A. M. Alkilany, O. C. Farokhzad, M. Mahmoudi, *Chem. Soc. Rev.* **2017**, *46*, 4218.
- [45] J. Zhao, M. H. Stenzel, *Polym. Chem.* **2018**, *9*, 259.
- [46] N. A. Franken, H. M. Rodermond, J. Stap, J. Haveman, C. van Bree, *Nat. Protoc.* **2006**, *1*, 2315.
- [47] X. Wang, H. Zhang, X. Chen, *Cancer Drug Resist.* **2019**, *2*, 141.
- [48] J. Maeda, C. E. Froning, C. A. Brents, B. J. Rose, D. H. Thamm, T. A. Kato, *PLoS One* **2016**, *11*, e0156689.
- [49] T. Dasgupta, D. A. Haas-Kogan, X. Yang, A. Olow, D. X. Yang, A. Gragg, L. A. Orloff, S. S. Yom, *Invest. New Drugs* **2013**, *31*, 1136.
- [50] J. A. Bonner, B. T. Vroman, T. J. H. Christianson, L. M. Karnitz, *Int. J. Radiat. Oncol. Biol. Phys.* **1998**, *42*, 921.
- [51] U. Kasid, S. Suy, P. Dent, S. Ray, T. L. Whiteside, T. W. Sturgill, *Nature* **1996**, *382*, 813.
- [52] P. Dent, A. Yacoub, P. B. Fisher, M. P. Hagan, S. Grant, *Oncogene* **2003**, *22*, 5885.
- [53] M. Chowdhary, K. R. Patel, H. H. Danish, D. H. Lawson, M. K. Khan, *OncoTargets Ther.* **2016**, *9*, 7149.
- [54] K. Meeth, J. X. Wang, G. Micevic, W. Damsky, M. W. Bosenberg, *Pigm. Cell Melanoma Res.* **2016**, *29*, 590.
- [55] P. Decuzzi, B. Godin, T. Tanaka, S. Y. Lee, C. Chiappini, X. Liu, M. Ferrari, *J. Controlled Release* **2010**, *141*, 320.
- [56] S. Shukla, F. J. Eber, A. S. Nagarajan, N. A. DiFranco, N. Schmidt, A. M. Wen, S. Eiben, R. M. Twyman, C. Wege, N. F. Steinmetz, *Adv. Healthcare Mater.* **2015**, *4*, 874.
- [57] A. Dash, M. R. Pillai, F. F. Knapp Jr, *Nucl. Med. Mol. Imaging* **2015**, *49*, 85.
- [58] K. Neyrinck, N. Breuls, B. Holvoet, W. Oosterlinck, E. Wolfs, H. Vanbilloen, O. Gheysens, R. Duellen, W. Gsell, I. Lambrichts, U. Himmelreich, C. M. Verfaillie, M. Sampaulesi, C. M. Deroose, *Theranostics* **2018**, *8*, 2799.
- [59] O. Keinanen, J. M. Brennan, R. Membreno, K. Fung, K. Gangangari, E. J. Days, C. J. Williams, B. M. Zeglis, *Mol. Pharm.* **2019**, *16*, 4416.
- [60] N. Pirooznia, K. Abdi, D. Beiki, F. Emami, S. S. Arab, O. Sabzevari, S. Soltani-Goshkhaneh, *Bioorg. Chem.* **2020**, *102*, 104100.
- [61] S. Poty, K. Mandleywala, E. O'Neill, J. C. Knight, B. Cornelissen, J. S. Lewis, *Theranostics* **2020**, *10*, 5802.
- [62] R. Bussani, F. De-Giorgio, A. Abbate, F. Silvestri, *J. Clin. Pathol.* **2007**, *60*, 27.
- [63] Y. Cui, J. D. Urschel, N. J. Petrelli, *Thorac. Cardiovasc. Surg.* **2001**, *49*, 35.
- [64] M. Hecht, L. Zimmer, C. Loquai, C. Weishaupt, R. Gutzmer, B. Schuster, S. Gleisner, B. Schulze, S. M. Goldinger, C. Berking, A. Forschner, P. Clemens, G. Grabenbauer, T. Muller-Brenne, J. Bauch, H. T. Eich, S. Grabbe, D. Schadendorf, G. Schuler, P. Keikavoussi, S. Semrau, R. Fietkau, L. V. Distel, L. Heinzerling, *Ann. Oncol.* **2015**, *26*, 1238.
- [65] P. Lu, Y.-L. Hsieh, *Carbohydr. Polym.* **2010**, *82*, 329.
- [66] B. Sun, M. Zhang, Q. Hou, R. Liu, T. Wu, C. Si, *Cellulose* **2016**, *23*, 439.
- [67] N. Amreddy, R. Muralidharan, A. Babu, M. Mehta, E. V. Johnson, Y. D. Zhao, A. Munshi, R. Ramesh, *Int. J. Nanomed.* **2015**, *10*, 6773.
- [68] M. H. Ullman-Cullere, C. J. Foltz, *Lab. Anim. Sci.* **1999**, *49*, 319.